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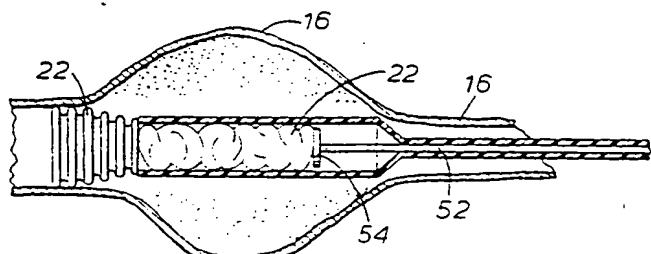
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㉓ Process and apparatus for restoring patency to body vessels.

㉔ A process in which a shape memory alloy, such as nitinol wire, which has been previously fabricated in its parent phase to form a longitudinally oriented coil of adjacent wire loops and thereafter cooled to its martensite phase and reshaped to a relatively straight shape, is utilised as an intraluminal device to reinforce a weakened or otherwise damaged vessel. The reformable wire is inserted into the vessel in such a manner to be temperature insulated such that, upon the removal of the insulation means, the wire reforms to its coil shape so as to be urged against the internal walls of the damaged vessel and supplies a patent channel through which body fluids may pass. In this manner, removal of the damaged portion of the vessel with the attachment of graft material as a replacement thereto along with the complex surgical techniques required to perform such is avoided.



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PROCESS AND APPARATUS FOR RESTORING
PATENCY TO BODY VESSELS

This invention relates to methods of treating
5 defects caused by a gunshot wound, stabbing, etc. or
where the vessel (artery, vein, or other body passage)
is perforated or disrupted. It is also particularly
adapted, but not limited, to reconstruction of an
abdominal aortic aneurysm.

10 Presently such aneurysms are surgically
corrected by the re-section thereof with accompanying
installation of a replacement graft. Generally this
graft is of a Dacron material constructed in
longitudinally expandible tubular form and is
15 surgically connected between the remaining portion of
the aorta and the left and right iliac arteries. Such
procedure is in detail described in an article set
forth on Figures 1 through 20, pages 231 through 233,
entitled "Resection of Abdominal Aortic Aneurysm"
20 published in the Atlas of Surgical Operations, 4th ed.
R. M. Zollinger and R. M. Zollinger, Jr. Such
procedure is time consuming, requires high skill and
involves a significant amount of patient risk. It
would, therefore, be highly desirable to replace such
25 technique with a simpler, less traumatic procedure
which is, accordingly, an object of the present

invention.

According to a first aspect of the present invention, a process of restoring the patency and/or re-establish continuity of a disrupted hollow body vessel which includes a localised defect disposed intermediate first and second patent vessel portions, characterised in inserting at least the forward end of a shape-memory alloy wire which has been previously fabricated in its parent phase to form a longitudinally oriented coil of adjacent wire loops and then cooled to its martensite phase and reshaped to an alternate form along the interior of said vessel past said defect to a position adjacent the first patent vessel portion while maintaining the temperature of said wire below its martensite transformation point and thereafter heating said wire to its transformation point so as to initially cause the thus reshaped wire loops of the forward wire to be urged against the interior of said first patent vessel portion so as to be at least temporarily positioned thereat and thereafter cause the reformation of the remainder of said coil so as to bridge said localised defect and into position adjacent said second patent vessel portion.

According to a second aspect of the present invention, apparatus for restoring the patency and/or re-establishing continuity of a disrupted hollow body

vessel which includes a localised defect disposed intermediate first and second patent vessel portions, characterised in that it comprises means for inserting at least the forward end of a length of shape-memory 5 alloy wire which has been previously fabricated in its parent phase to form a longitudinally oriented coil of adjacent wire loops and then cooled to its martensite phase and reshaped to an alternate form along the interior of said vessel past said defect to a position 10 adjacent the first patent vessel portion, tube means for temporarily maintaining the temperature of said wire below its martensite transformation temperature point and means for progressively withdrawing said tube from said body.

15 In order that the invention may be more readily understood, it will now be described, by way of example only, with reference to the accompanying drawings, in which:-

20 Figure 1 is a partial sectional view showing the restoration of a body vessel, namely, the aorta having an aneurysm therein with the procedure and devices of the present invention in an initial stage;

Figure 2 is a view similar to Figure 1 but showing an intermediate stage;

25 Figure 3 shows the completed procedure;

Figure 4 is a partial sectional view taken

through line 4-4 of Figure 3;

Figure 5 is a view similar to Figure 1 but showing a modified form of the invention wherein a fabric graft is not utilised;

5 Figure 6 is a view similar to Figure 2 but showing an intermediate stage;

Figure 7 is a partial sectional view of another form of the invention in a partially completed stage; and

10 Figure 8 is a view similar to Figure 7 but showing the completed repair structure.

Turning now to the drawings, and more particularly Figures 1 through 3, 5 and 6 thereof, the present invention will be explained in relationship to 15 the repair of an aortic aneurysm. It should be understood, however, that the present invention has utility not only as a reinforcement of a weakened arterial wall, such as the aortic aneurysm shown, but also in the restoration of patency to previously narrowed, weakened, ballooned, or otherwise defective or impaired lumen or other body channels. Such body channels may include arteries, the esophagus, bile ducts, uretha, trachea, and the like. Other specific uses to which the procedures described in the present 20 invention include the repair or correction of the following:

1. intraluminal lining of AAA or iliac or femoral aneurysms;
2. recanalisation of injured vessels caused by blunt or penetrating trauma;
- 5 3. dilation and recanalisation of stenotic arterial segments;
4. tamponade and obliteration of bleeding esophageal varices;
5. recanalisation of esophageal stenoses
- 10 secondary to carcinoma or benign strictures;
6. dilation and recanalisation of biliary stenoses secondary to strictures, tumours and cancer of pancreas and common bile duct;
8. ureteral strictures and tracheal strictures.

15 It should also be understood that the above use list is not intended to be exclusive and that any body vessel which has been narrowed, weakened, or in another way requires a reinforcement may be subject to the present invention. Also as utilised therein, the term vessel is used in a general sense to include body channels including, but not limited to, artery, esophagus, bile duct, uretha, trachea, and the like, and that the term body includes not only humans but animals as well.

20 25 One form of the present invention is illustrated in Figures 1 through 4, wherein an aortic

aneurysm is shown being repaired by the procedure shown by the progressive drawing sequence of Figures 1 through 3. Therein, an aneurysm 10 is depicted intermediate patent proximal or first and distal or 5 second portions 12, 14 of the aorta 16. The lining of the aneurysm 10 includes clotted blood material or plaque 18 which in turn reduces the effective passage of arterial blood through the aorta and increases the chance of clotted material entering the blood stream 10 and causing damage elsewhere in the body.

A hollow sheath 20 is shown inserted, as by conventional techniques, into the aorta 16 from the distal side thereof, as shown to the right of Figure 1, and positioned so as to be adjacent the proximal side 15 of the aneurysm 10 but well within the patent portion 12 thereof, (distal and proximal refer to positioning relative to the heart, that is, remote from and close to, respectively). A fabric graft 22 is positioned within the sheath 20 and is selected to be of an 20 adequate longitudinal extent so as to adequately span the aneurysm 10, that is, to contact patent vessel portions 12 and 14 on opposite sides of such aneurysm. The sheath 20 may include an enlarged proximal end 50 to accommodate the folded or bunched together, etc. 25 graft structure 22. Such graft 22 may take the form of those currently utilised in full surgical techniques

such as previously referred to in the Zollinger et al publication and utilised to at least in part illustrate the state of the prior art prior to the present invention. Such Dacron or other synthetic or natural material graft may be accordian pleated such that its overall length is shortened when introduced, then expanded as will hereinafter be more fully explained so as to span the full extent of the aneurysm.

A shape memory metal alloy wire is attached to the graft 22 at least at its proximal end and may be attached at a plurality of longitudinally spaced locations along such graft. The wire 24 is of an alloy such as nitinol which exhibits anthropomorphic qualities of memory and trainability and are commonly referred to as shape-memory alloys. If such alloys are plastically deformed at one temperature, they will completely recover to their original shape on being raised to a higher temperature. A discussion and identification of such alloys is set forth in the article by L. McDonald Shetky entitled "Shape-Memory Alloys" at pages 74 through 82 of Vol. 241 (5) Nov. 1979 Scientific American. A further discussion of such alloys, and particularly nickel-titanium alloys commonly referred to as nitinol, is set forth in the publication "A Source Manual for Information on Nitinol and NiTi", First Revision, by David Goldstein, Research

and Technology Department, 1 February 1980, Naval Surface Weapons Center, Dahlgren, Virginia 22448 (NSWC TR 80-59).

In the present invention, a nitinol wire 24 which has been alloyed to exhibit a martensite transformation temperature somewhat below the normal body temperature range is satisfactory. Such wire is shaped by known techniques into the form of a continuous coil 26. The individual loops 28 are disposed in adjacent but spaced relationship to each other while in a parent phase and thereafter cooled so as to produce a martensite crystalline form and thereafter reshaped so as to form a relatively straight length of continuous wire. The wire 24 is maintained in such condition by maintaining the temperature thereof below its martensite transformation temperature of approximately 37° in this case. The manner in which said wire is attached to the graft 22 may be by conventional techniques such as sewing and the like.

In this regard, it should be pointed out that when the wire resumes its coiled form after being internally positioned in the body vessel, in this case the aorta 16, it will if appropriately attached to the graft 22 expand such graft longitudinally. Accordingly, a leading portion of the wire 24 is attached to the graft and thereafter if desired at points along the length of

the wire such that several continuous loops may be formed between such attachment points. The wire intermediate such attachment points may be compressed or bunched so as to be conveniently housed with the 5 proximal portion 50 of the insulating sheath 20.

Such sheath 20 is preferably formed of an insulating plastic resinous material such as polyethylene and the like and is of sufficient thickness so as to maintain the temperature of the wire 10 24 below its martensite transformation point during the insertion of the sheath into the desired position within the aorta. Such position is upstream of the aneurysm 10 (proximal to the heart) and generally 15 adjacent thereto but well within the extent of the first patent portion 12 of the aorta 16. Thereafter, the sheath 20 is initially withdrawn a short distance so as to expose a portion of the lead portion of the wire and graft 22 such that the wire is exposed to the heat of the surrounding body tissue and permitted to reach 20 and exceed the martensite transformation phase and, accordingly, initiate reformation into its coiled form. In this regard, it should be pointed out that the diameter of the coil as initially formed is approximately equal to or slightly greater than that of 25 the normal internal diameter of the patent aorta portions 12 and 14 such that the individual loops 28 of

the coil 26 urge the graft material 22 snugly against the patent portions of the aorta 16 so as to ensure a positive position therein, as shown in Figure 2. Thereafter the remainder of the insulation sheath is 5 progressively removed such that the entire reformation of the coil takes place with the attendant longitudinal extension of the graft 22. The interior of the sheath may be fitted with a relatively stiff member 52, i.e. a wire rod or rod-like element, having a platform 54 10 attached at its proximal end and positioned within the enlarged sheath head 50. The member 52 may include a thumb ring 56 at its distal end such that the surgeon may more easily manipulate and thus position the sheath 20 as by inserting his or her thumb through ring 56 and 15 grasping the distal end of the sheath 20 by a flange 58 provided thereat.

Also the diameter of the coil is preferably such that it approximates the normal internal extent of the aorta such that the passage of blood therethrough 20 may be normal. Also where appropriate, the flow of blood through the aorta is temporarily shunted by conventional means such as the insertion of an inflatable catheter if required or desirable in regard 25 to the heating and shaping memory characteristics of the wire 24 or to assist in the initial positioning and/or expansion of the wire.

It may thus be seen that the overall objectives of the present invention are carried out by the above-described novel procedure and such is accomplished without full surgical techniques and with 5 a minimum possibility of dislodging clotted material from the aneurysm 10 into the blood stream.

Turning now to Figures 5 and 6 of the drawing, a modified form of the invention is shown wherein the fabric graft 22 of the previously described embodiment has been omitted. In that regard, the 10 formation of the coil 26a is such that the individual loops 28a thereof are very closely spaced so as to approach or actually physically touch each other. Otherwise, the procedure as previously described in the 15 embodiment of Figures 1 through 4 is essentially the same, that is, an insulating sheath 20 carrying the wire 24a is projected into the vessel and thereafter the sheath slightly withdrawn such that the wire initially expands into a partial coil form and to 20 directly contact the internal surface of the first patent aorta portion 12 and thereafter progressively withdrawn so as to bridge the aneurysm 10 in the same manner as previously described and thereafter come into positioning contact with the second patent portion 14. 25 The wire in this embodiment need not, however, be bunched so as to be positioned essentially entirely

within the graft but may include only forward portions of such positioned in the sheath. Thus the wire 24a can be of the relatively straight form shown and have a significant extent projecting rearwardly out of the 5 sheath and patient's body. In this embodiment, it is also possible to use a sheath of reduced diameter approaching even that of the wire. Furthermore, the wire may actually be moved relative to a stationary sheath so as to project outwardly of the lead end of 10 the sheath so as to firmly position the wire vis-a-vis the patent vessel portion 12 or even to initiate heating and thus reformation of the wire in this matter.

It should also be understood that a procedure 15 combining the techniques and constructions shown and described in the Figures 1 through 4 and Figures 5 and 6 embodiments may be used as when a graft to which the wire is attached only to its leading or proximal end is used. Therein the member 52 may be utilised and 20 constructed to be hollow (tubular) such that the wire 24 or 24a can pass internally through it outwardly into the enlarged sheath head 50 through an opening (not shown) provided in the platform 54. Also this combined technique could also be of use when a bunched wire 24 25 or 24a is placed in the sheath head 50 yet further wire is desired to follow and as an aid in initially moving

the wire bunch relative to the sheath to initiate position.

Turning now to Figures 7 and 8 of the drawing, the present process is shown in directing a 5 constricted vessel 30 such that the constriction is forced to more natural or at least patent dimensions by the application of the techniques of the present invention. In such case, a wire 34 which may correspond to either the wire 24 or 24a of the 10 previously explained embodiments may be utilised. Such wire 34 is positioned on one side of the constriction 32 by a sheath 20 and thereafter heated to its martensite transformation point and then enabled to progressively reshape itself to its original coil form 15 38 so as to progressively force the walls of the vessel into an original or at least patent position. A length of graft material can also be used in conjunction with the process, as shown in Figures 7 and 8.

It should be understood that heating the wire 20 in any of the above embodiments to its transformation temperature could be accomplished other than solely by conduction and convection from the body but by infrared and radiation. Thus infrared waves could be directed at forward portions of the wire by known means so as to 25 progressively heat and reform the wire. Also when the body temperature is not exclusively relied upon as the

source of heat for the wire, its reformation temperature could be increased above body temperatures if necessary or desirable to achieve particular characteristics. Naturally, radiation heating could 5 also be utilised in conjunction with the previously described embodiments. Also although the wire form has been illustrated in the form of side-by-side circular loops along the longitudinal coil extent, it should be understood that the loops could extend back and forth 10 longitudinally and progressively build up in a circular path to form the completed wire form (cylindrical).

While there is shown and described herein certain specific structure embodying this invention, it 15 will be manifest to those skilled in the art that various modifications and rearrangements of the parts may be made without departing from the spirit and scope of the underlying inventive concept and that the same is not limited to the particular forms herein shown and 20 described except insofar as indicated in the scope of the appended claims.

Claims:

1. A process of restoring the patency and/or re-establish continuity of a disrupted hollow body vessel which includes a localised defect disposed intermediate first and second patent vessel portions, characterised in inserting at least the forward end of a shape-memory alloy wire (24) which has been previously fabricated in its parent phase to form a longitudinally oriented coil (26), (38) of adjacent wire loops and then cooled to its martensite phase and reshaped to an alternate form (24a) along the interior of said vessel past said defect to a position adjacent the first patent vessel portion (12) while maintaining the temperature of said wire below its martensite transformation point and thereafter heating said wire to its transformation point so as to initially cause the thus reshaped wire loops (28) of the forward wire end to be urged against the interior of said first patent vessel portion (12) so as to be at least temporarily positioned thereat and thereafter cause the reformation of the remainder of said coil so as to bridge said localised defect (18) and into position adjacent said second patent vessel portion (14).

2. The process as claimed in claim 1,
characterised in that said heating is progressive in
the direction from the first and to the second portion.

5 3. The process as claimed in claim 2,
characterised in that the martensite transformation
temperature of said wire is below the normal
temperature range of said body.

10 4. The process as claimed in any preceding
claim, characterised in that said heating of said wire
takes place by said body.

15 5. The process as claimed in claim 3 or 4,
characterised in that the temperature of said wire is
regulated by insulating means when initially inserted
into said vessel.

20 6. The process as claimed in claim 5, wherein
said insulating means is a tube through which said wire
is transported to said first patent vessel portion
after which said tube is progressively withdrawn.

7. The process as claimed in claim 1,
characterised in that the adjacent loops of said
reformed coil are closely spaced to each other so as to
essentially form the wall of the vessel in said
5 defective portion thereof.

8. The process as claimed in claim 1,
characterised in that a tubular graft is positioned
between said reshaped coil and the interior wall of
10 said vessel.

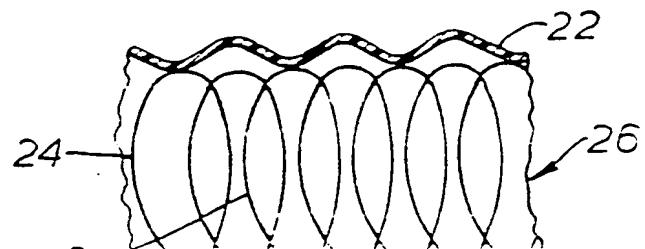
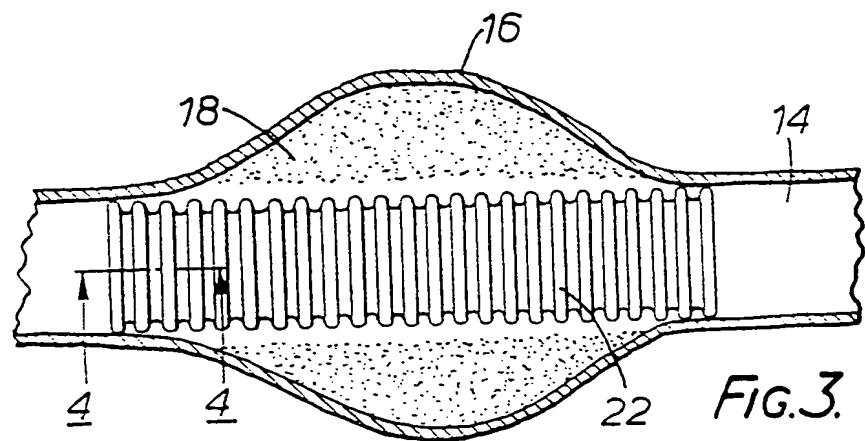
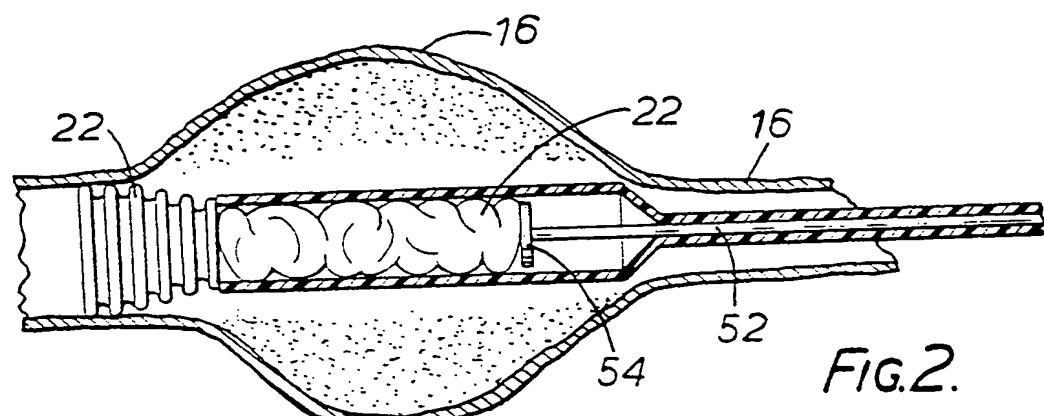
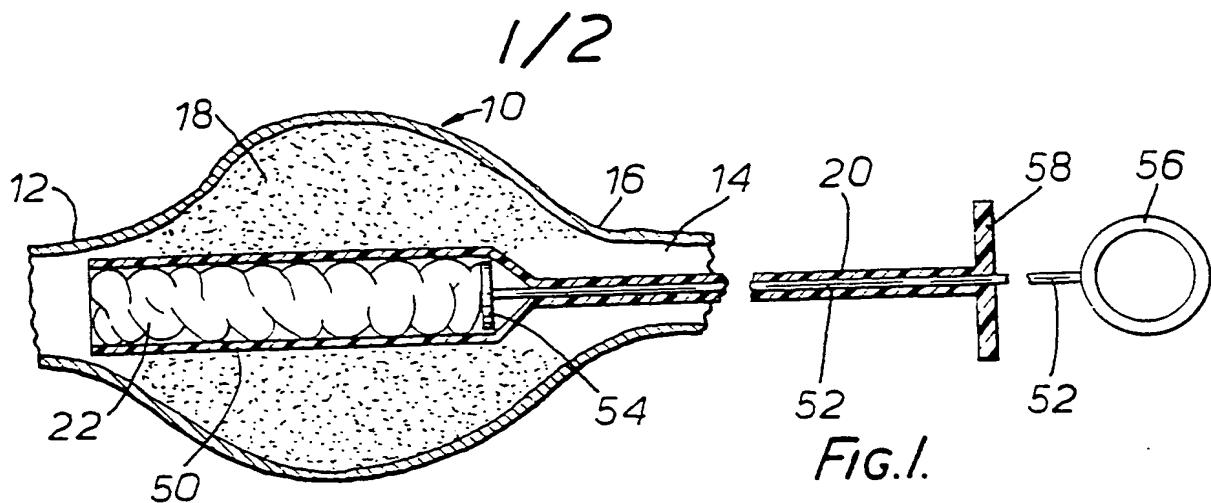
9. The process as claimed in claim 8 as
 appended to claim 6, characterised in that said wire is
 attached to said graft at least at the forward end
 5 thereof and said wire and graft are temporarily
 positioned in said tube in a crushed compacted form.

10. The process as claimed in claim 3,
characterised in that said wire is composed of a
20 nitinol alloy.

11. The process as claimed in any preceding
claim, characterised in that said alternate wire form
is a relatively straight length thereof.

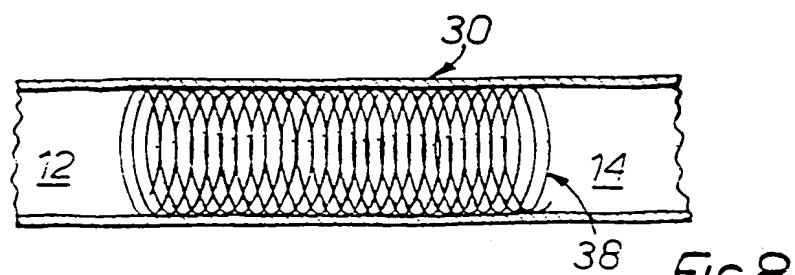
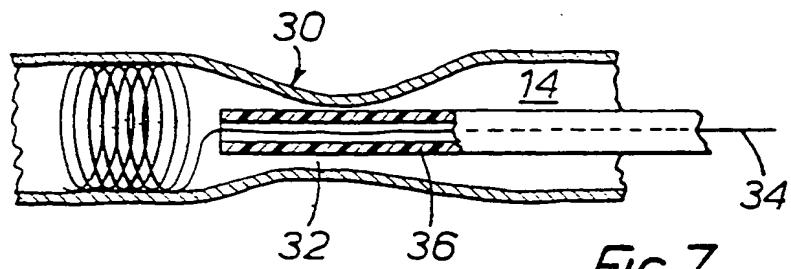
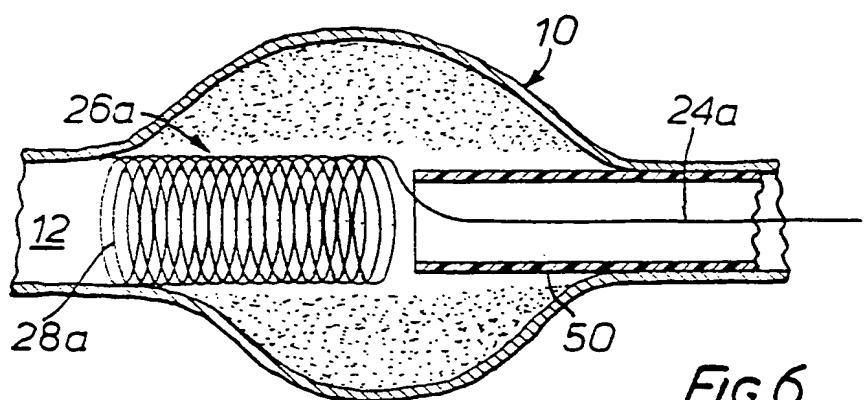
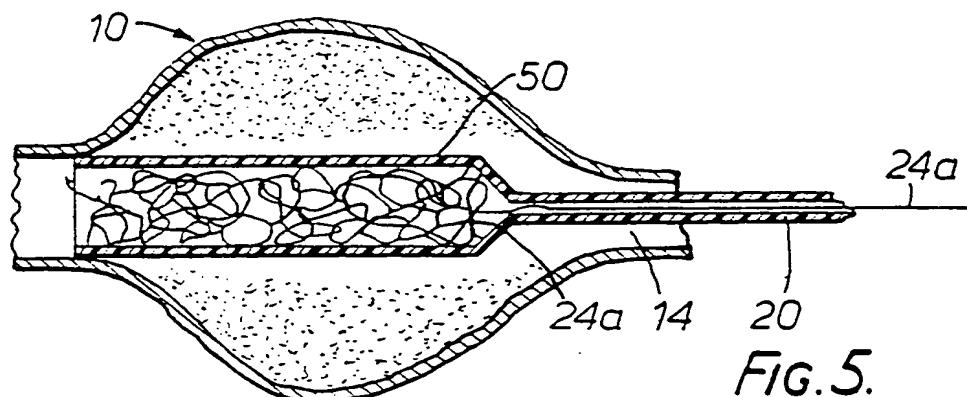
12. Apparatus for restoring the patency and/or re-establishing continuity of a disrupted hollow body vessel which includes a localised defect disposed intermediate first and second patent vessel portions,
5 characterised in that it comprises means for inserting at least the forward end of a length of shape-memory alloy wire which has been previously fabricated in its parent phase to form a longitudinally oriented coil of adjacent wire loops and then cooled to its martensite
10 phase and reshaped to an alternate form along the interior of said vessel past said defect to a position adjacent the first patent vessel portion, tube means for temporarily maintaining the temperature of said wire below its martensite transformation temperature
15 point and means for progressively withdrawing said tube from said body.

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